



# Integrating AC-Electric Fields into the Cell Microenvironments

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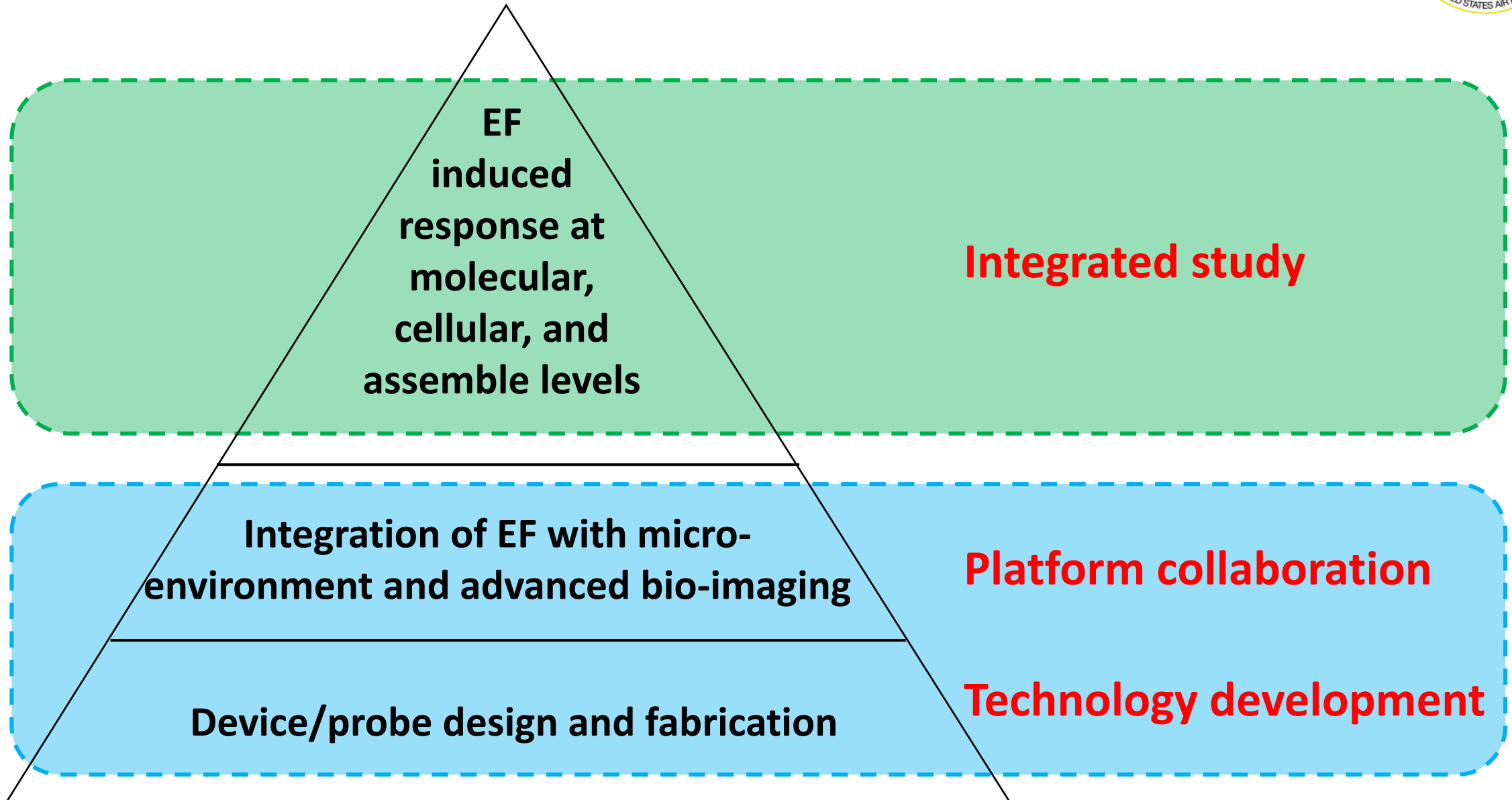
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John Albeck (UC Davis)

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Wolfgang Losert (UMD), John Fourkas (UMD), Budri Sharif (John Hopkins), Peter  
Devreotes (John Hopkins), Patrick Kanold (UMD)



# Overview: Our role in this MURI project





## Synergetic activities:

- **Visits to UCDavis** (4 times). Each visit took one week with fully scheduled experiments
  - Prof. Min Zhao, Dr. Liang Guo, Prof. John G. Albeck at UC Davis
- **Visits to UMD** (3 times). Each visit took one week with fully scheduled experiments, and **joint discussions with UMD and John Hopkins** (1 day).
- Extensive preparation through online meetings and emails among all groups before each visit
  - Identify key scientific questions
  - Design experiment plans
  - Prepare samples and protocols
- **Customized chips and electronic controllers shared among MURI groups** with quick turn around time to meet specific requirements in collaborative studies
- **Introduced new cell lines** from UCDavis and UMD **to ASU**
- Built **bioimaging platform with environmental control systems** at ASU with help from UCDavis and UMD.
- **Biweekly web conference discussion between ASU and UCDavis**
  - Tracking progress
  - Discussion on data analysis
  - Preparation of manuscript
- **Regular discussion with all MURI team members** through web conference to receive additional comments and suggestion



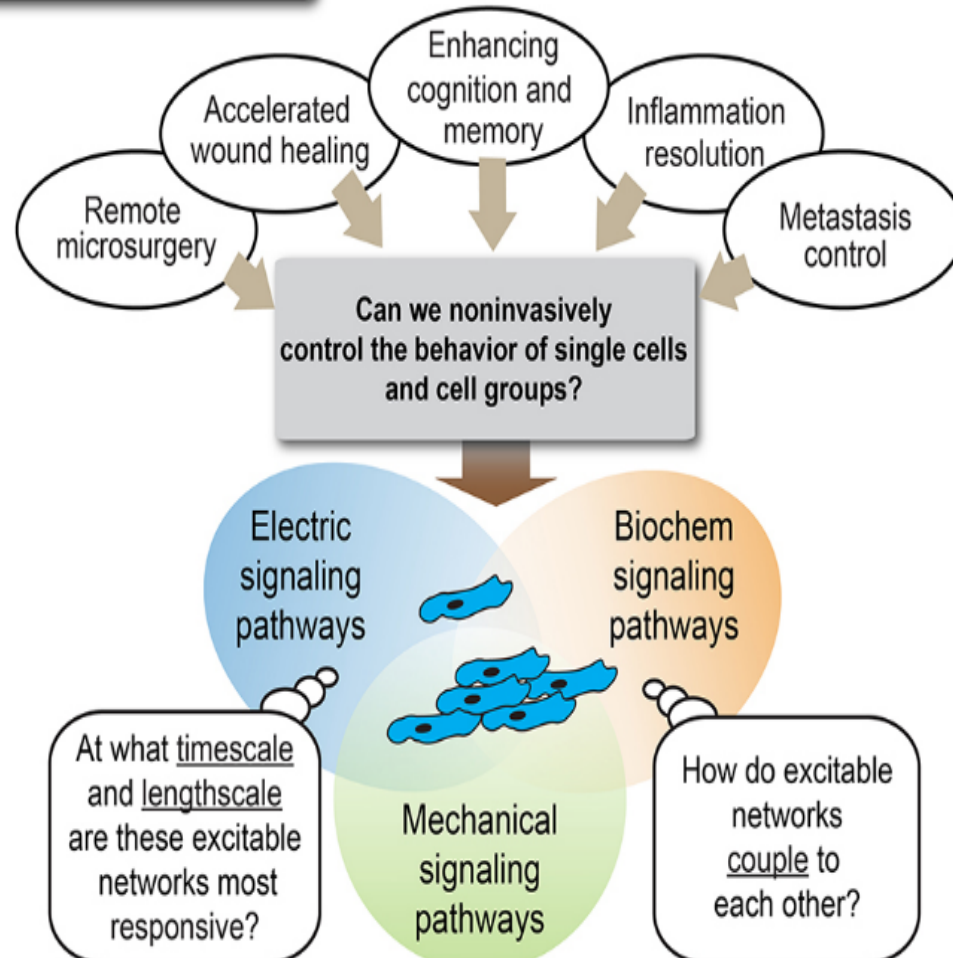


# Our interest



Combining **spatiotemporally modulated electric field stimuli** with biochemical and mechanical signals to study **intra-/inter-cellular signaling network** couplings

## Objective and Impact



### Electric Field:

- Polarized field – direct interaction on charges and dipoles
- Localized – high spatial resolution
- Accurate timing – high temporal resolution

### Biochemical stimuli:

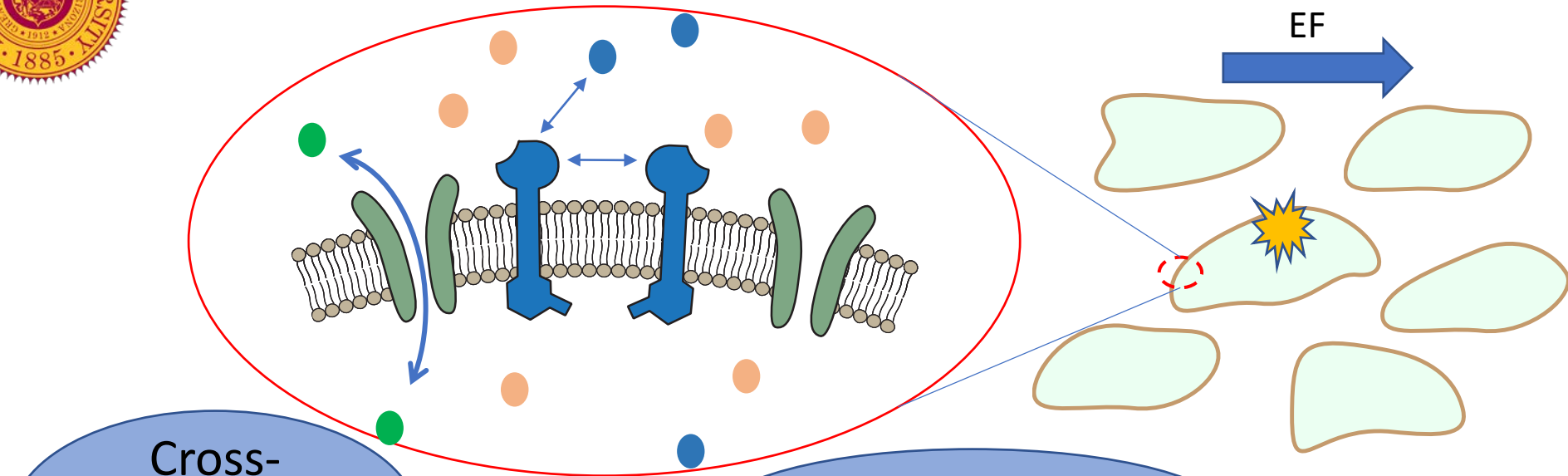
- Rich toolbox
- Highly specific
- Molecular level information
- Typically can only apply to a group of cells – low spatial resolution
- Gradient change is usually slow – low temporal resolution

### Mechanical stimuli:

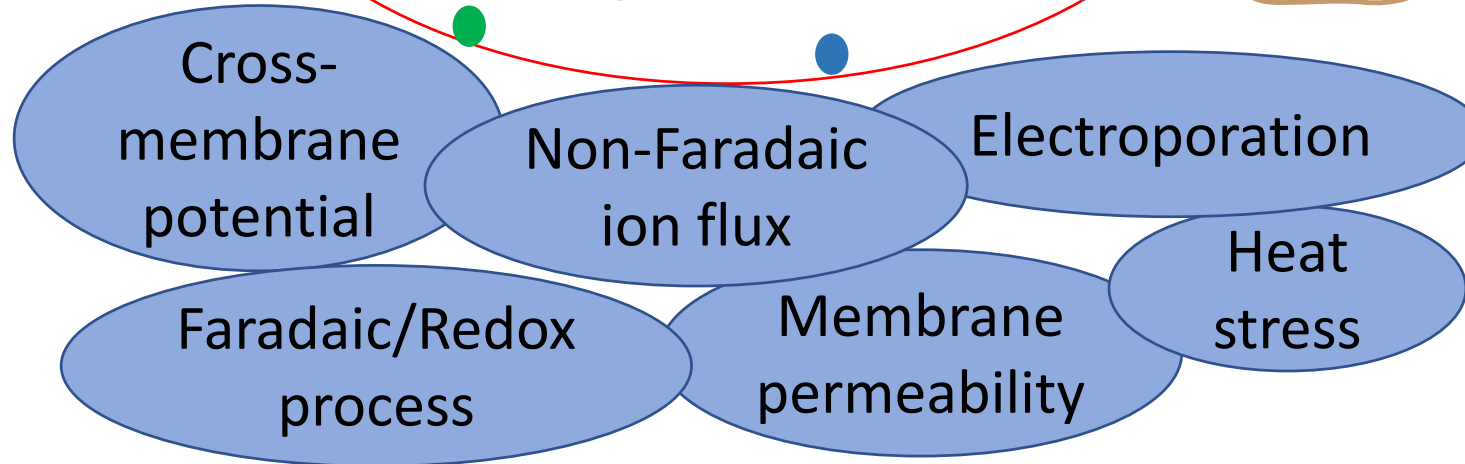
- Typically static patterns, passive stimulation only
- Can achieve subcellular spatial resolution
- Distinct behavioral consequence



# A lot of things can happen when EF is applied to a cell



- Heterogeneity
- Intercellular communication
- Coordinated behaviors



- Global environment change
- Multiple signaling pathways involved
- Long time scale
- Large length scale (diffusion and inter-cellular process could be involved)

- Changes of binding energy/kinetics at the membrane
- EF-dipole, EF-charge interactions of membrane protein/lipid domains
- Others?

- **Localized?**
- **Time scale?**
- **Frequency dependency?**
- **Specificity?**

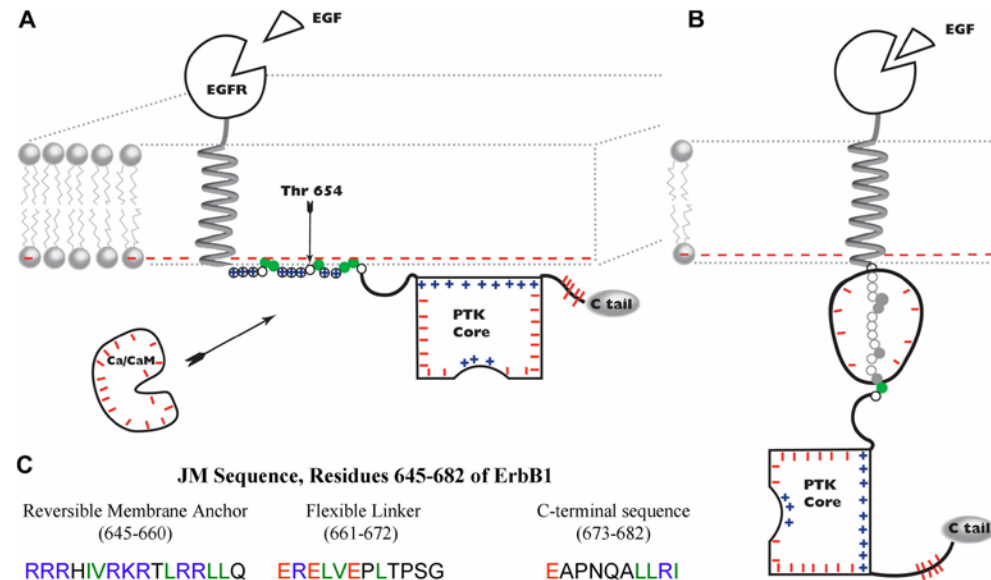


# Hypothesis and predictions



- **Direct, specific EF modulation at molecule level without chemical complication**
  - We hypothesize that AC EF could modulate the electrostatic interactions of proteins or other biomolecules at the cell membrane interface, leading to functional conformational changes
- **Predictions:**
  - Highly specific to membrane protein
  - Threshold behavior
  - Time scale ( $0.1 \mu\text{s} \sim 1 \text{ ms}$ ?)
  - Frequency dependent

**How do we separate/distinguish direct EF interaction from other effects?**



McLaughlin S, et. al, *J. Gen. Physiol.* 126(1):41–53.

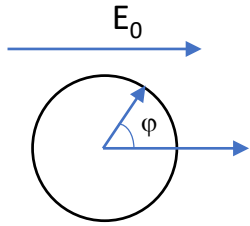
Charge/dipole  
interactions



Conformational  
changes



# EF at the cell membrane depends on frequency

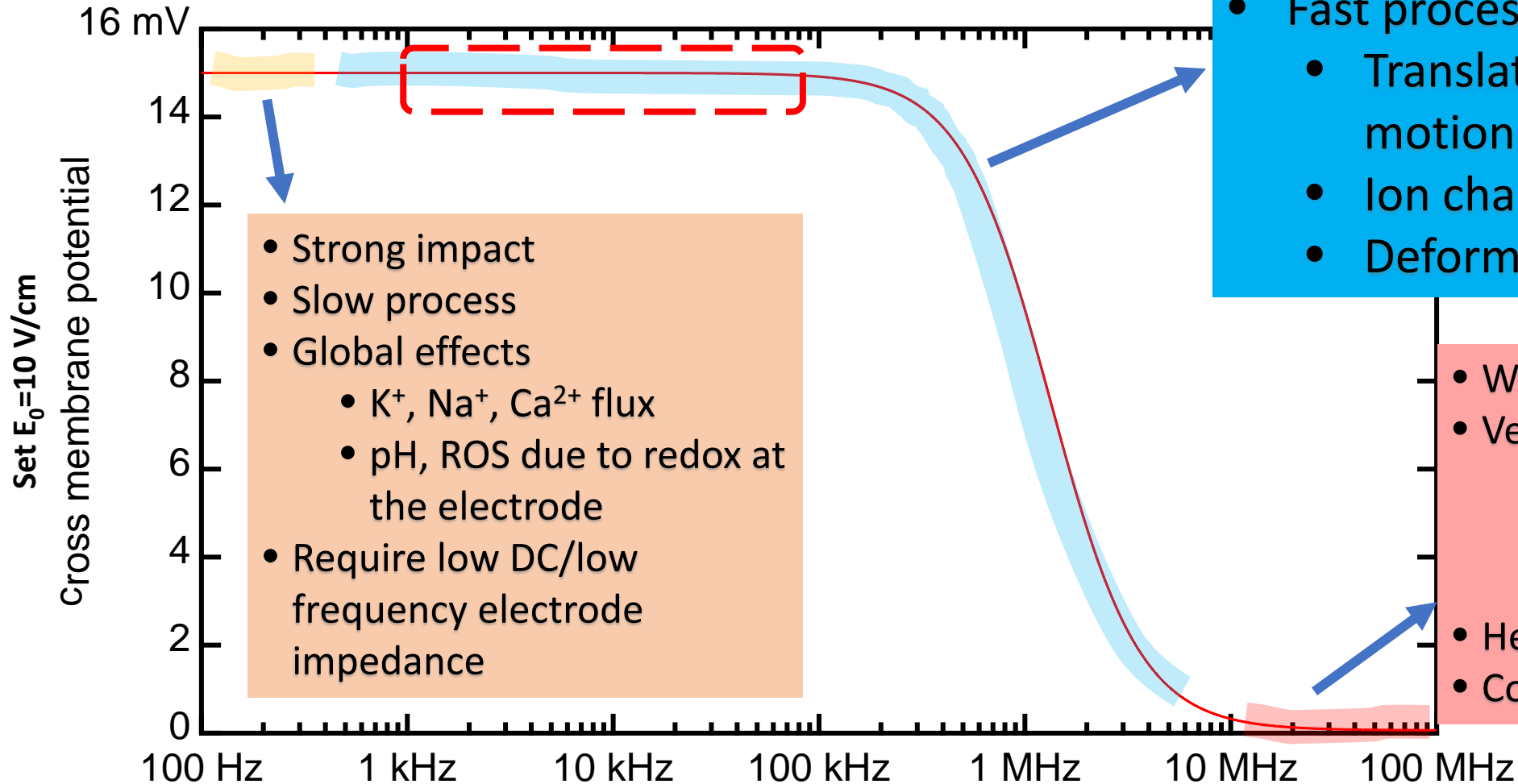


$$\psi(j\omega) = \frac{3}{2} E_0 R \cos \varphi \frac{1}{1 + j\omega \tau_m}$$

$$\text{Where } \tau_m = RC_m \left( \frac{1}{\sigma_1} + \frac{1}{2\sigma_e} \right)$$

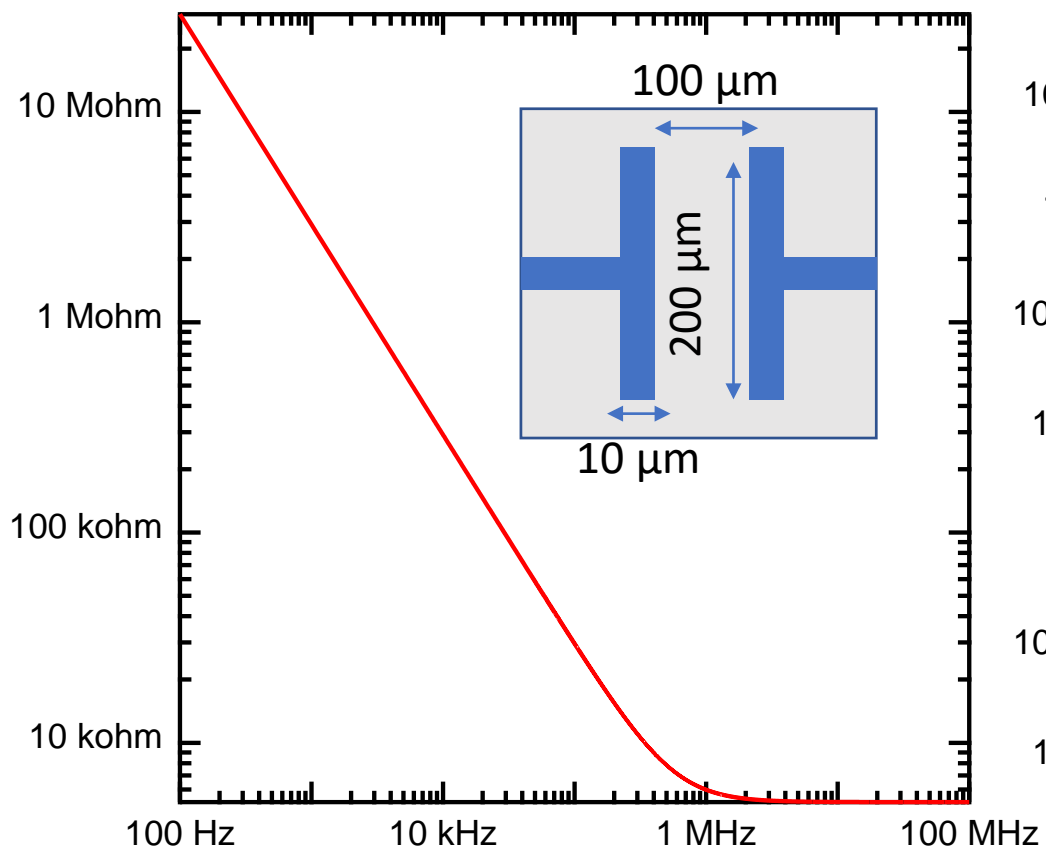
$$\psi(j\omega) = \frac{3}{2} E_0 R \cos \varphi \frac{1 + j\omega \tau_{m2}}{1 + j\omega \tau_{m1}}$$

$$\text{Where } \tau_{m1} = \frac{\epsilon_m}{\frac{d}{2\sigma_e\sigma_1} + \sigma_m}, \tau_{m2} = \frac{\epsilon_1 + 2\epsilon_e}{\sigma_1 + 2\epsilon_e}$$

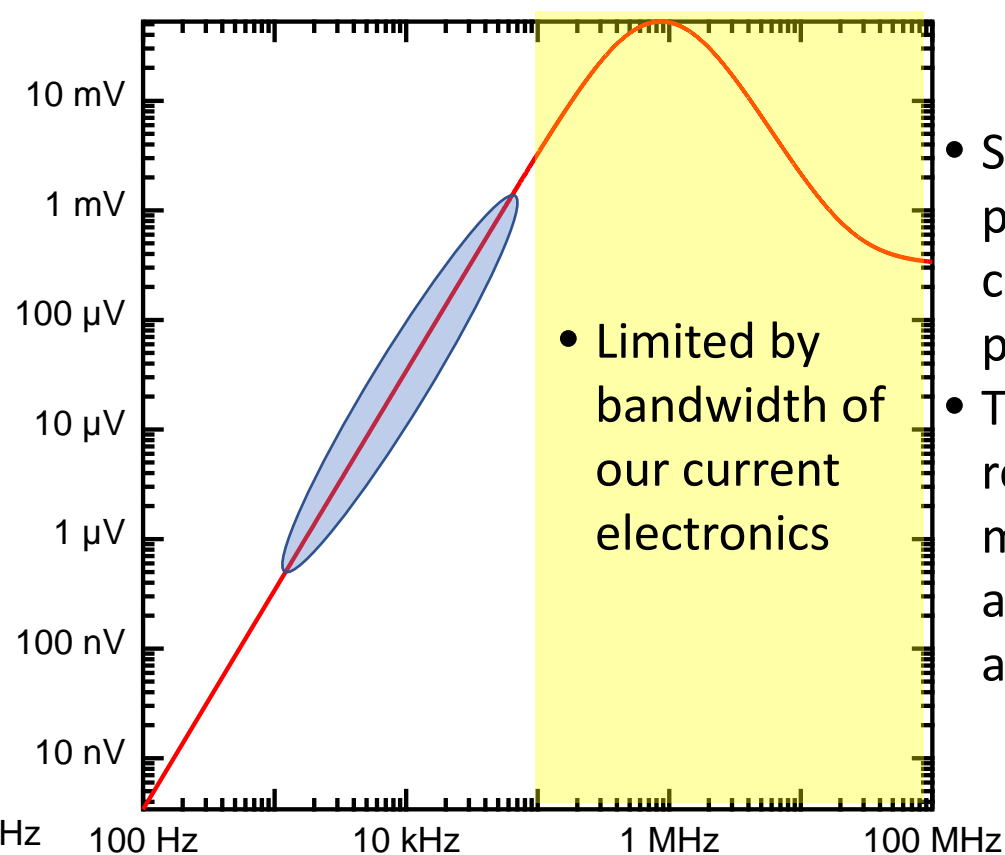




# Impedance of microelectrodes and the cell membrane together provide a band-pass of AC EF



Impedance of microelectrodes – high pass of signals

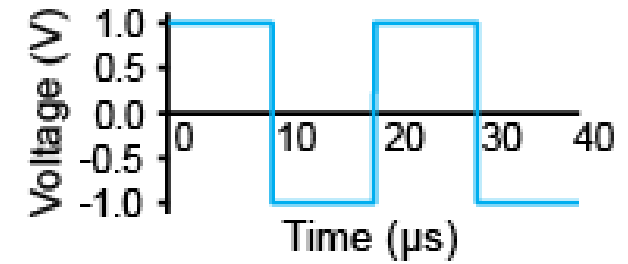
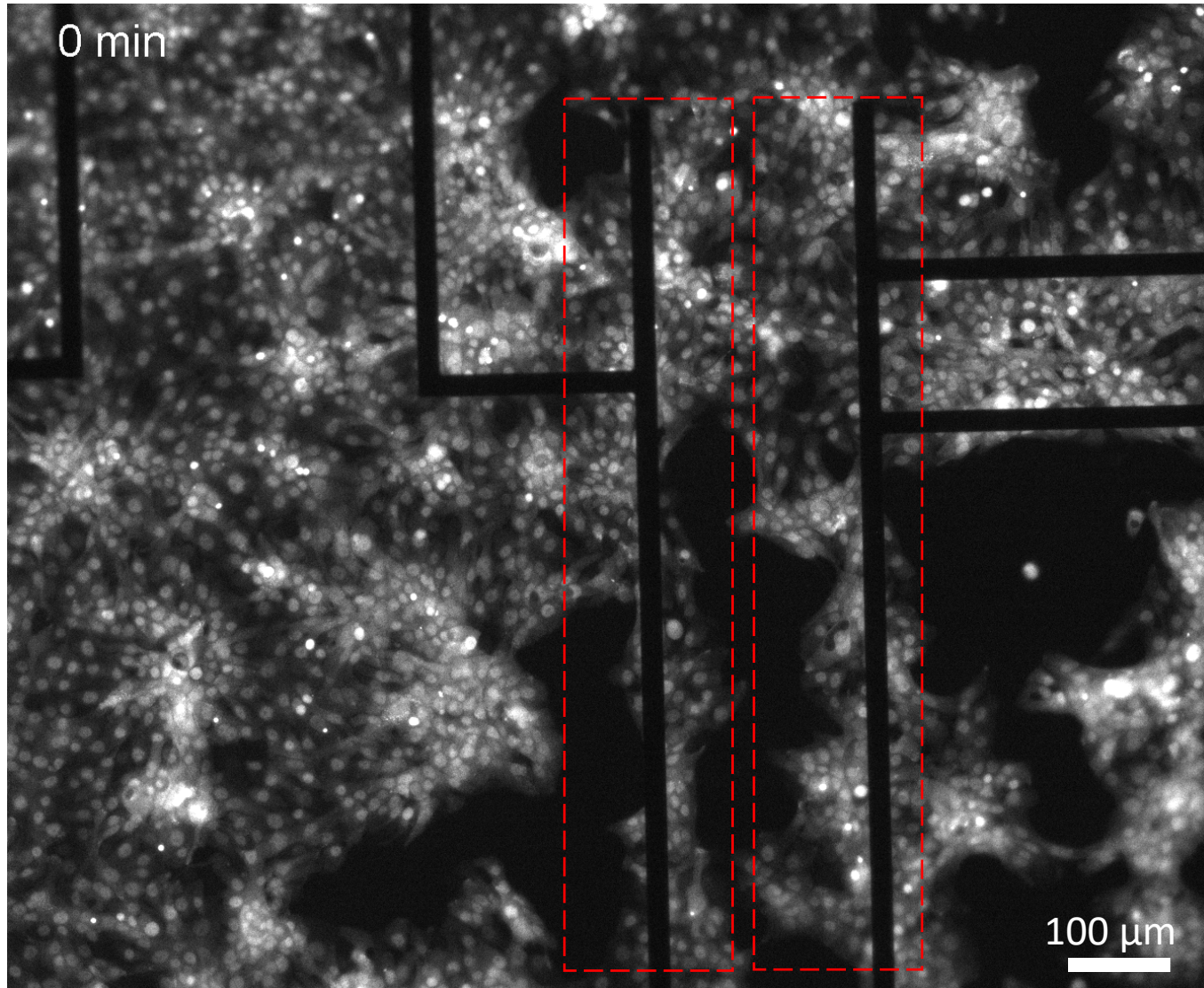


Simulation of cross-membrane potential when applying  $\pm 1$  V AC bias at the microelectrode pairs

- Limited by bandwidth of our current electronics
- Significant perturbation of cross-membrane potential
- Time scale ( $\mu\text{s}$ ~ $\text{ms}$ ) relevant to membrane protein and ionic channel activities



# A showcase: Surprising observation of localized AC EF activation of ERK in MCF10A cells



- Reproducible, non-invasive, and highly localized **ERK activation by bipolar AC EF pulses**
- **Threshold** of activation: nominal EF strength 10~100V/cm
- **Faradaic process excluded** at the electrode/cell interface



Houpu Li  
ASU



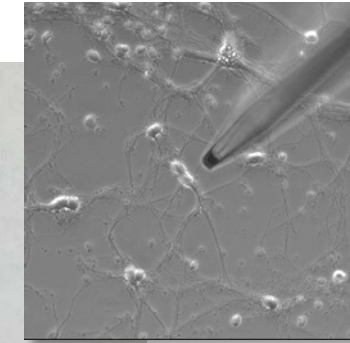
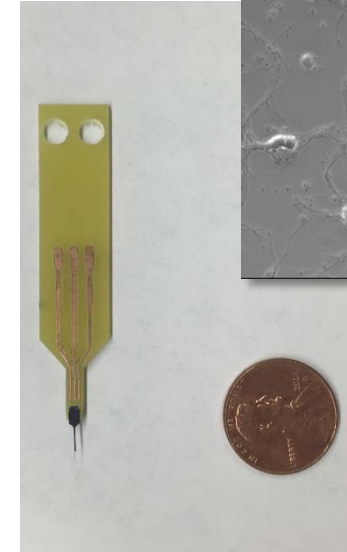
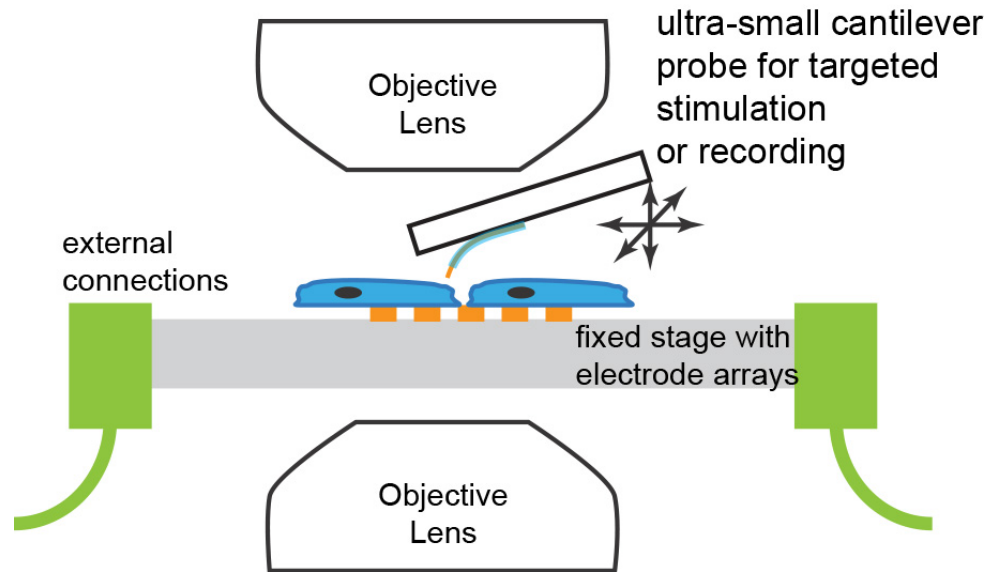
Liang Guo  
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Yuan Wang  
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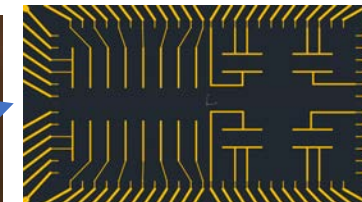
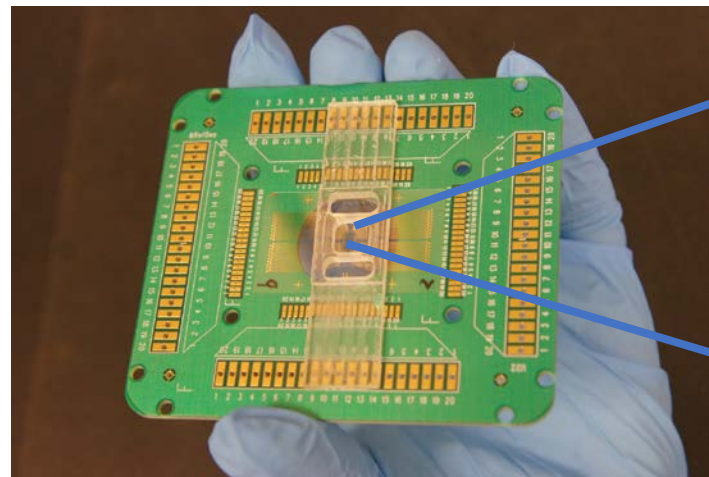
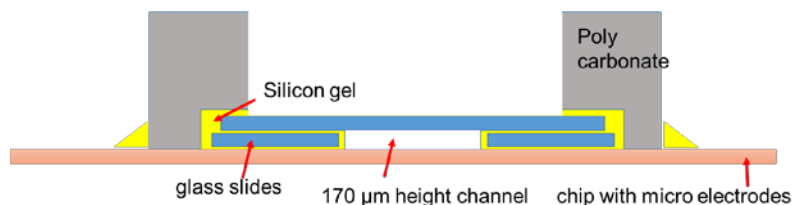


# Microelectrode Arrays and Freestanding probes provide highly localized EF delivery to cells, allowing **sub-cellular level spatial resolution**

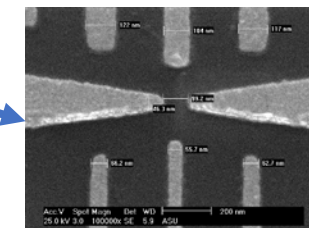


- Freestanding probe for accurately targeted sub-cellular EF stimulation

We have utilized UC Davis experience in their petridish-based system, and designed a chamber that can be assembled around our chips to give optimal delivery of global EF, and imaging capability.



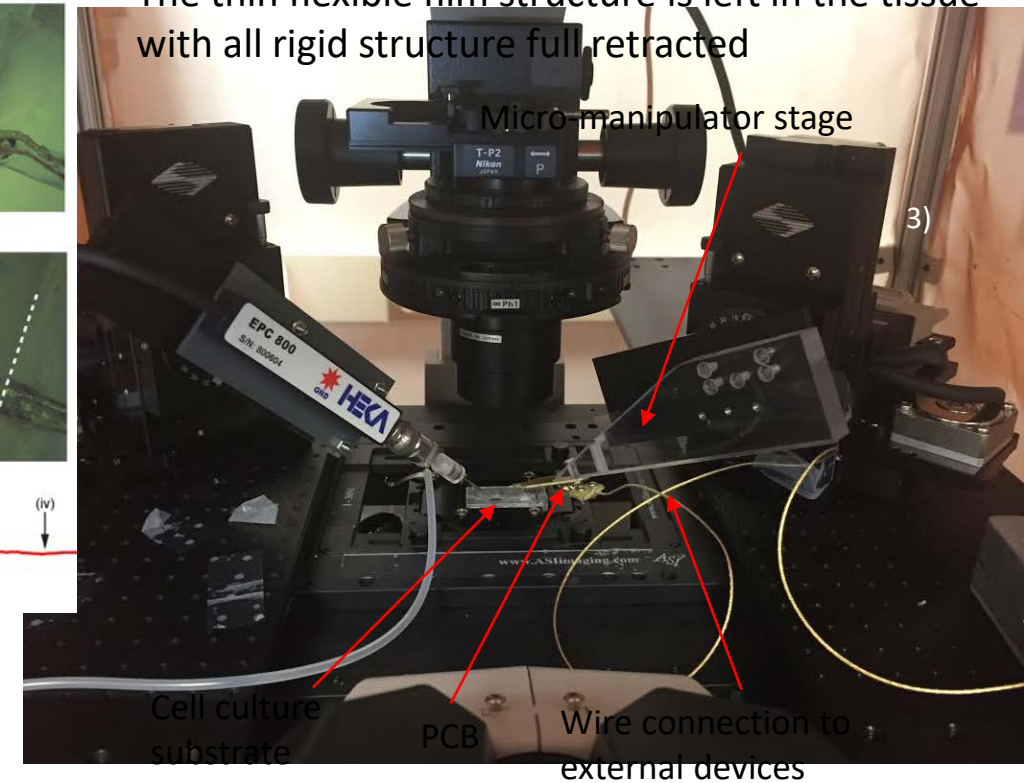
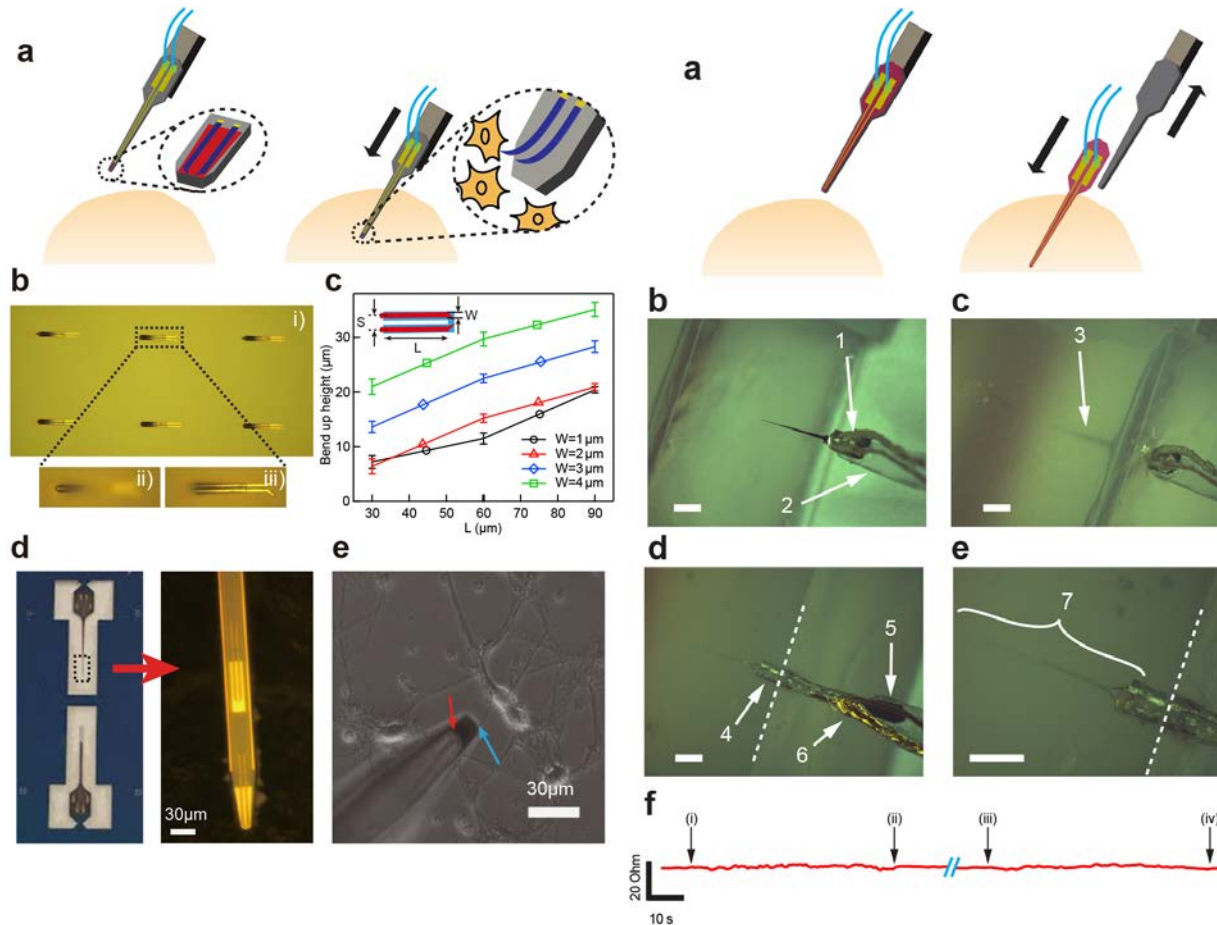
- Surface microelectrode arrays for cellular level EF stimulation



- Surface nanoelectrodes for subcellular level EF stimulation

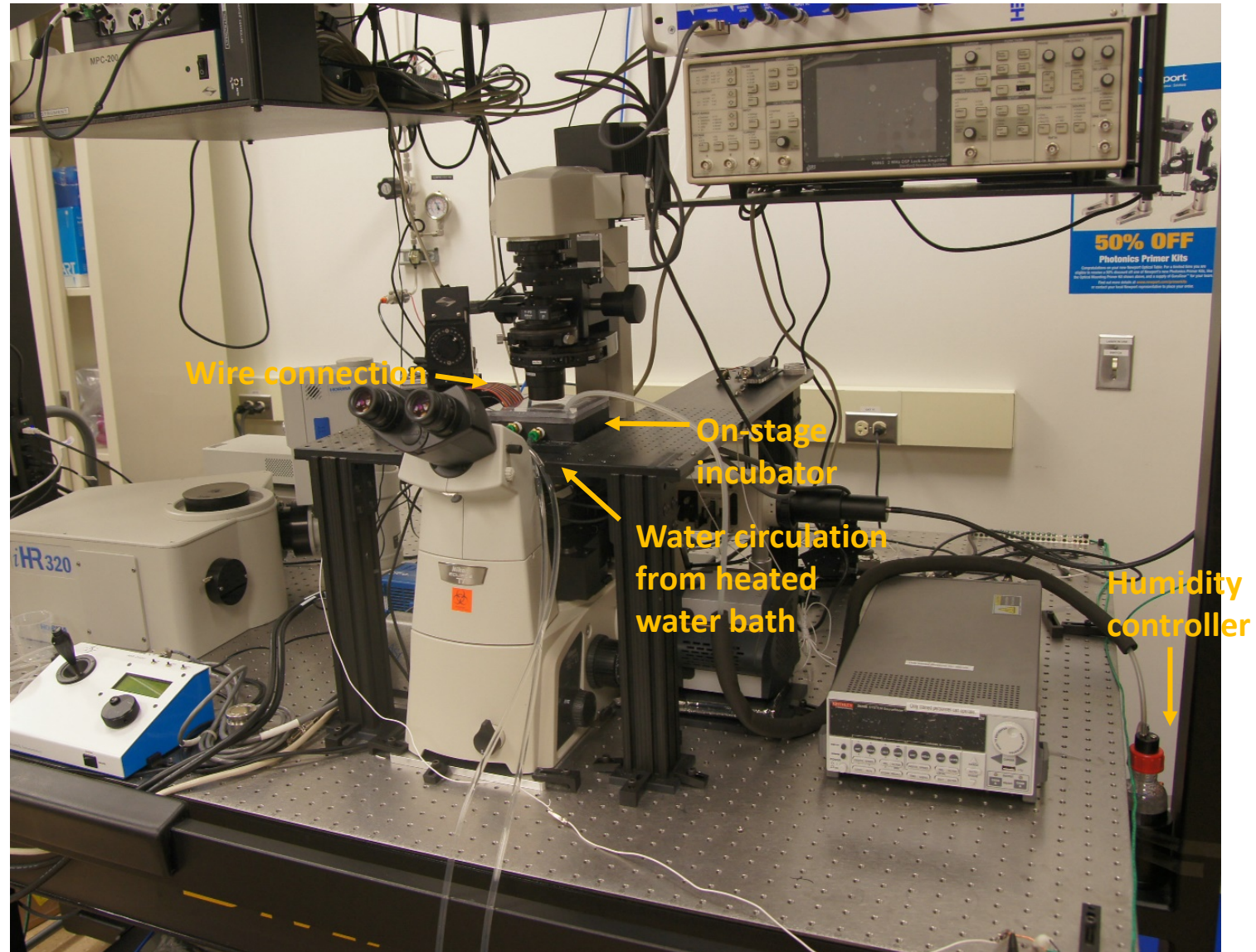
# Ultra-small freestanding probe: accurate targeting individual cells

- The whole top device layer is build within flexible polymer
- The backbone silicon structure is used only for surgically deliver the probe accurately into deep tissue
- The biologically degradable sacrificial layer dissolves within 20-30 minutes after the insertion
- The thin flexible film structure is left in the tissue with all rigid structure full retracted





## EF stimulation and imaging system built at ASU



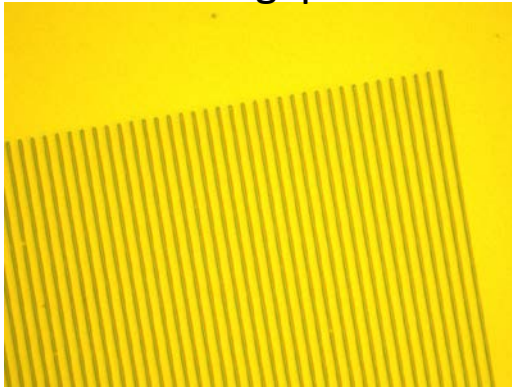


# Integrating local EF with mechanical stimuli

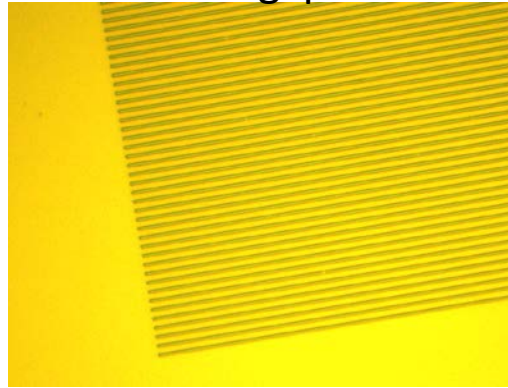
We need to define topological features with high spatial resolution and accurate alignment with electrode edges.



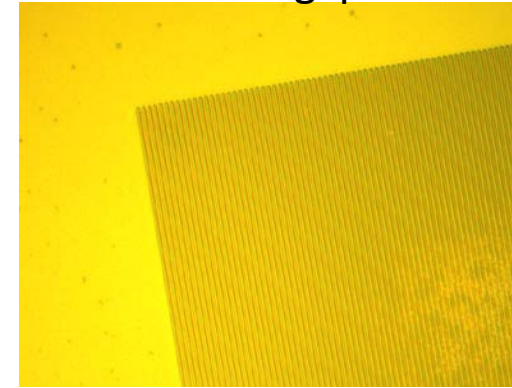
3 um gap



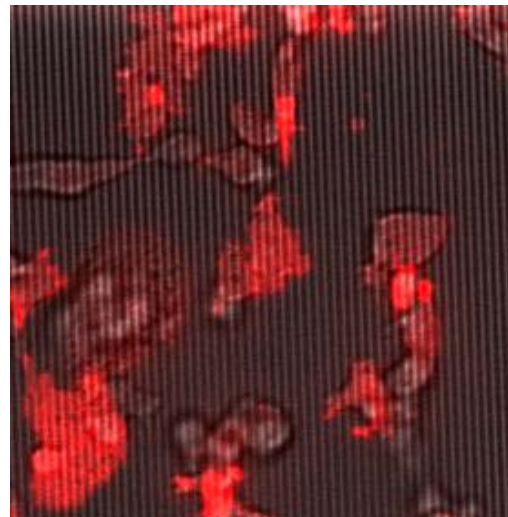
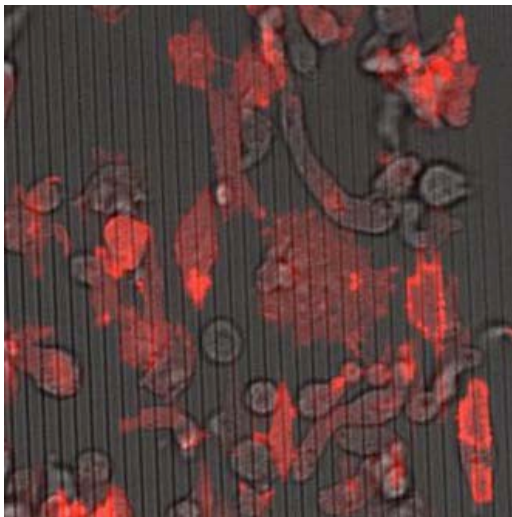
2 um gap



1 um gap



0.5 um thick SU8 stripes with 0.7 um width and different gap sizes



These SU8 stripes can provide good guidance to dicty cell migrations.